

# The GH-Method

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## **Viscoelastic and Viscoplastic Glucose Theory Applications (VGT #45): Applying the Physics Concepts of Viscoelasticity and Viscoplasticity to Estimate the “Difference of Relative Energy Level” Measured by the Hysteresis Loop Area, a Biophysical and Engineering Phenomenon, Along with the Carbs/Sugar Intake Grams, a Biomedical-Related Key Lifestyle Detail, from Inputs of Three Distinctive PPG Ranges to Provide a Guesstimated Damage Level of Internal Organs Resulted from Hyperglycemia Based on the GH-Method: Math-Physical Medicine (No. 630)**

Gerald C. Hsu\*

eclairMD Foundation, USA

**Note:** Readers who want to get a quick overview can read the abstract, results, and graphs.

### **Abstract**

Recently, the author applied theories of viscoelasticity and viscoplasticity from engineering and physics along with wave theory and energy theory from physics to conduct his biomedical research on output biomarkers of postprandial plasma glucose (PPG), which is one of the key indicators for diabetes, resulting from the input biomarker of carbs/sugar intake amounts, which is a major cause for hyperglycemia. In this article, he extracted three sub-groups of PPG waveforms and datasets during a long period of ~4 years from 5/8/2018 to 3/16/2022. All of the PPG data are collected via a continuous glucose monitoring (CGM) sensor device at 15-minute time intervals (96 data each day) over 1,408 days and 4,310 meals that contain 56,030 PPG data. These three PPG sub-groups are listed below: Low PPG - 2,885 meals with 6.6 carbs/sugar grams and 122 mg/dL average PPG; Medium PPG - 1,298 meals with 23.9 carbs/sugar grams and 132 mg/dL average PPG; High PPG - 127 meals with 73.7 carbs/sugar grams and 153 mg/dL average PPG. There are three specific calculation steps for the numerical operation. In the first step, he applies the theories of viscoelasticity and viscoplasticity to generate their stress values using strain rate (PPG change rate) multiplied by the average carbs/sugar grams to plot the stress-strain diagram. He defines his biomedical strain and stress as follows: Strain =  $\epsilon$  = individual output biomarker value (PPG) at present time (each 15-minutes interval). Stress =

$\sigma = (d\epsilon/dt) * \eta = (d\text{-strain}/d\text{-time}) * \eta = ((\text{PPG at present time} \cdot \text{PPG at previous time}) / 15) * \text{viscosity factor } (\eta: \text{average carbs/sugar grams})$ , where the time duration of 15 was chosen due to PPG measurements taken at 15-minute intervals. In the second step, he calculates the three enclosed areas of the stress-strain curve, an engineering term for “hysteresis loop”, using the formula of the trapezoid area. This loop area can be used as an estimated “relative energy” associated with three different carbs/sugar ranges: 0-15g, 15-50g, and 50-200g. This hysteresis loop area is formed by both PPG and PPG change rate \* carbs/sugar. Therefore, conceptually, this loop-enclosed area can be used as a measurement tool for the total energy associated with both force (PPG rate \* carbs/sugar) and deformation (PPG). PPG itself contributes around 41% (sensor eAG) to 75% (finger eAG) and is a key component of HbA1C value. Furthermore, the PPG change rate is equivalent to the glucose fluctuation (GF) or the glycemic variability (GV) which have been proven to connect with diabetes conditions closely. In the third step, he combined these three datasets for a final comparison. Due to his definition of stress as the multiplication of the strain change rate with carbs/sugar grams, where the PPG strain itself is also strongly influenced by carbs/sugar intake amount. So, this stress-strain diagram has double-counted the influences from the carbs/sugar element, one explicitly and the other implicitly. Therefore, he compares the three carbs/sugar

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\*Corresponding author: Gerald C. Hsu, eclairMD Foundation, USA

ratios first and then calculates the specific ratio of the hysteresis loop area ratio versus the carbs/sugar ratio. These three calculated ratios can be visually observed and compared clearly from one combined chart with three separate stress-strain diagrams using the same scales for the x-axis and y-axis. To offer a simple explanation to readers who do not have a physics or engineering background, the author includes a rather brief excerpt from Wikipedia regarding the description of basic concepts for elasticity and plasticity theories, viscoelasticity, and viscoplasticity theories from the disciplines of engineering and physics in the method section. In summary, a clear conclusion can be drawn as follows: “A higher glucose amount generates higher energy which causes more damage to internal organs through blood flow”. This simple conclusive statement can be easily understood and accepted by medical professionals, except for the word “energy”. However, by using the author’s math-physical medicine (MPM) research methodology, it can offer a concise comprehension of this complex biomedical picture with sound theoretical proof and detailed data. By delving into this picture closely, we can discover additional findings as explained below. However, the author wants to state the following key conclusive statement first: “Energy required to cause material failure, such as organ damage, can be represented through the total area under the stress-strain curve (hysteresis loop) which indicates the energy per unit volume of glucose”. (1) The low PPG sub-group behaves like an elastic and pseudo viscoelastic pattern since its ending strain (PPG at 120 mg/dL) is almost the same as its starting strain (PPG at 121 mg/dL). Incidentally, the low PPG data are time-dependent. The author selects the extremely low average carbs/sugar intake amount of 6.6 grams from his 2,885 meals (67% of his total 4,310 meals) as its corresponding viscosity factor ( $\eta$ ). (2) The medium PPG group acts like an elastic and perfect viscoelastic pattern since its ending strain is identical to its starting strain (both PPG at 126 mg/dL). Incidentally, the medium PPG data are also time-dependent. The author selects a higher but moderate average carbs/sugar intake amount of 23.9 grams from his 1,298 meals (30% of his total 4,310 meals) as its corresponding viscosity factor ( $\eta$ ). (3) The high PPG group behaves like a plastic and viscoplastic pattern since its ending

strain (PPG at 152 mg/dL) is much higher than the starting strain (PPG at 129 mg/dL). On the high PPG stress-strain curve, there is a huge opening which is a very different shape from the other two subgroups’ “closed loops”. Even the high PPG data is also time-dependent. The author selects the extremely high average carbs/sugar intake amount of 73.7 grams (3% of his total 4,310 meals) as its corresponding viscosity factor ( $\eta$ ). (4) From the three separate stress-strain diagrams, we can see three calculated hysteresis loop areas: 1.6 for the low PPG group, 12.2 for the medium PPG group, and 93.3 for the high PPG group. Therefore, combined with the contribution percentage of meals distribution, the total “effective loop area” is:  $1.6*0.67+12.2*0.3+93.3*0.03 = 1.072+3.66+2.799 = 7.531$  Energy required to cause material failure, such as organ damage, can be represented through the total area under the stress-strain curve (hysteresis loop) which indicates the energy per unit volume of glucose. This effective loop area of 7.531 is slightly higher than the medium PPG subgroup with 23.9 grams of carbs/sugar and 132 mg/dL of averaged PPG. He should definitely avoid having high PPG (hyperglycemic) situations. (5) The three comparing ratios for low PPG, medium PPG, and high PPG are: loop area ratios = 1:8:58; carbs/sugar ratios = 1:4:11; ratio of area/carbs = 1:2:5. The three comparisons through different ratios are expressed with a “relative scale of comparison”. It should be noted that the high loop area is caused by the combined effect of the high strain (PPG) and high stress (high PPG change rate with high carbs/sugar), high glucose fluctuation (GF), or high glycemic variability (GV). From the author’s previous research results and other published papers, the high GF or GV indeed causes damage to internal organs. From the relativity of curve shape, data value, and hysteresis loop area of the individual diagram and the combined chart of the three stress-strain diagrams, the following statement can be made based on the above findings: the high PPG group not only has higher values of PPG, GF, and GV but also carry a higher level of energy circulating inside the body through blood flow. The high level of energy is the primary source (other than viruses or infections) that cause different types of internal damage to the body organ cells which leads to various chronic disease complications.

**Keywords:** Viscoelasticity; Viscoplasticity; postprandial plasma glucose; diabetes

**Abbreviations:** PPG: postprandial plasma glucose; GF: glucose fluctuation; GV: glycemic variability; MPM: math-physical medicine

## 1. INTRODUCTION

Recently, the author applied theories of viscoelasticity and viscoplasticity from engineering and physics along with wave theory and energy theory from physics to conduct his biomedical research on output biomarkers of postprandial plasma glucose (PPG), which is one of the key indicators for diabetes, resulting from the input biomarker of carbs/sugar intake amounts, which is a major cause for hyperglycemia.

In this article, he extracted three sub-groups of PPG waveforms and datasets during a long period of ~4 years from 5/8/2018 to 3/16/2022. All of the PPG data are collected via a continuous glucose monitoring (CGM) sensor device at 15-minute time intervals (96 data each day) over 1,408 days and 4,310 meals that contain 56,030 PPG data. These three PPG sub-groups are listed below:

Low PPG - 2,885 meals with 6.6 carbs/sugar grams and 122 mg/dL average PPG;

Medium PPG - 1,298 meals with 23.9 carbs/sugar grams and 132 mg/dL average PPG;

High PPG - 127 meals with 73.7 carbs/sugar grams and 153 mg/dL average PPG

There are three specific calculation steps for the numerical operation.

In the first step, he applies the theories of viscoelasticity and viscoplasticity to generate their stress values using strain rate (PPG change rate) multiplied by the average carbs/sugar grams to plot the stress-strain diagram. He defines his biomedical strain and stress as follows:

Strain

=  $\epsilon$

= individual output biomarker value (PPG) at present time (each 15-minutes interval)

Stress

=  $\sigma$

=  $(d\epsilon/dt) * \eta$

=  $(d\text{-strain}/d\text{-time}) * \eta$

=  $((\text{PPG at present time} - \text{PPG at previous time}) / 15) * \text{viscosity factor } (\eta: \text{average carbs/sugar grams})$

Where the time duration of 15 was chosen due to PPG measurements taken at 15-minute intervals.

In the second step, he calculates the three enclosed areas of the stress-strain curve, an engineering term for “hysteresis loop”, using the formula of the trapezoid area. This loop area can be used as an estimated “relative energy” associated with three different carbs/sugar ranges: 0-15g, 15-50g, and 50-200g.

This hysteresis loop area is formed by both PPG and PPG change rate \* carbs/sugar. Therefore, conceptually, this loop-enclosed area can be used as a measurement tool for the total energy associated with both force (PPG rate \* carbs/sugar) and deformation (PPG). PPG itself contributes around 41% (sensor eAG) to 75% (finger eAG) and is a key component of HbA1C value. Furthermore, the PPG change rate is equivalent to the glucose fluctuation (GF) or the glycemic variability (GV) which have been proven to connect with diabetes conditions closely.

In the third step, he combined these three datasets for a final comparison. Due to his definition of stress as the multiplication of the strain change rate with carbs/sugar grams, where the PPG strain itself is also strongly influenced by carbs/sugar intake amount. So, this stress-strain diagram has double-counted the influences from the carbs/sugar element, one explicitly and the other implicitly. Therefore, he compares the three carbs/sugar ratios first and then calculates the specific ratio of the hysteresis loop area ratio versus the carbs/sugar ratio. These three calculated ratios can be visually observed and compared clearly from one combined chart with three separate stress-strain diagrams using the same scales for the x-axis and y-axis.

To offer a simple explanation to readers who do not have a physics or engineering background, the author includes a rather brief excerpt from Wikipedia regarding the description of basic concepts for elasticity and plasticity theories, viscoelasticity, and viscoplasticity theories from the disciplines of engineering and physics in the method section.

## 2. METHODS

### 2.1 Brief introduction of math-physical medicine (MPM) research

The author has collected ~3 million data regarding his health condition and lifestyle details over the past 12 years. He spent the entire year of 2014 developing a metabolism index (MI) model using topology concept, nonlinear algebra, algebraic geometry, and finite element method. This model contains various measured biomarkers and recorded lifestyle details along with their induced new biomedical variables for an additional ~1.5 million data. Detailed data of his body weight, glucose, blood pressure, heart rate, blood lipids, body temperature, and blood oxygen level, along with important lifestyle details, including diet, exercise, sleep, stress, water intake, and daily life routines are included in the database. There is a total of 10 categories covering approximately 500 detailed elements that constitute his defined “metabolism model” which are the building blocks or root causes for diabetes and other chronic disease complications, including but not limited to cardiovascular disease (CVD), chronic heart disease (CHD), stroke, chronic kidney disease (CKD), retinopathy, neuropathy, foot ulcer, and hypothyroidism. The end result of the MI development work is a combined MI value within any selected period with 73.5% as the dividing line between a healthy and unhealthy state. The MI serves as the foundation for many of his follow-up medical research work.

During the period from 2015 to 2017, he focused his research on type 2 diabetes (T2D), especially glucoses, including fasting plasma glucose (FPG), postprandial plasma glucose (PPG), and estimated average glucose (eAG), and hemoglobin A1C (HbA1C). During the following period from 2018 to 2022, he concentrated on researching medical complications resulting from diabetes, chronic diseases, and metabolic disorders which include heart problems, stroke, kidney problems, retinopathy, neuropathy, foot ulcer, diabetic skin fungal infection, hypothyroidism, diabetic constipation, cancer, and dementia. He has also developed a few mathematical risk models to calculate the probability percentages of developing various diabetic complications.

From his previous medical research work, he has identified and learned that the associated energy of hyperglycemic conditions is the primary source causing many diabetic complications which lead to death. Therefore, a thorough knowledge of the energies is important to achieve a better understanding of the dangerous complications.

### 2.2 Elasticity, plasticity, viscoelasticity and viscoplasticity

The difference between elastic materials and viscoelastic materials (from “Soborthans, innovating shock and vibration solutions”).

What are elastic materials?

Elasticity is the tendency of solid materials to return to their original shape after forces are applied on them. When the forces are removed, the object will return to its initial shape and size if the material is elastic.

What are viscous materials?

Viscosity is a measure of a fluid’s resistance to flow. A fluid with large viscosity resists motion. A fluid with low viscosity flows. For example, water flows more easily than syrup because it has a lower viscosity. High viscosity materials might include honey, syrups, or gels – generally things that resist flow. Water is a low viscosity material, as it flows readily. Viscous materials are thick or sticky or adhesive. Since heating reduces viscosity, these materials don’t flow easily. For example, warm syrup flows more easily than cold.

What is viscoelastic?

Viscoelasticity is the property of materials that exhibit both viscous and elastic characteristics when undergoing deformation. Synthetic polymers, wood, and human tissue, as well as metals at high temperature, display significant viscoelastic effects. In some applications, even a small viscoelastic response can be significant.

Elastic behavior versus viscoelastic behavior

The difference between elastic materials and viscoelastic materials is that viscoelastic materials have a viscosity factor and the elastic ones don’t. Because viscoelastic materials have the viscosity factor, they have

a strain rate dependent on time. Purely elastic materials do not dissipate energy (heat) when a load is applied, then removed; however, a viscoelastic substance does.

The following brief introductions are excerpts from Wikipedia:

“Elasticity (physics):

The physical property when materials or objects return to original shape after deformation.

In physics and materials science, elasticity is the ability of a body to resist a distorting influence and to return to its original size and shape when that influence or force is removed. Solid objects will deform when adequate loads are applied to them; if the material is elastic, the object will return to its initial shape and size after removal. This is in contrast to plasticity, in which the object fails to do so and instead remains in its deformed state.

The physical reasons for elastic behavior can be quite different for different materials. In metals, the atomic lattice changes size and shape when forces are applied (energy is added to the system). When forces are removed, the lattice goes back to the original lower energy state. For rubbers and other polymers, elasticity is caused by the stretching of polymer chains when forces are applied.

Hooke's law states that the force required to deform elastic objects should be directly proportional to the distance of deformation, regardless of how large that distance becomes. This is known as perfect elasticity, in which a given object will return to its original shape no matter how strongly it is deformed. This is an ideal concept only; most materials which possess elasticity in practice remain purely elastic only up to very small deformations, after which plastic (permanent) deformation occurs.

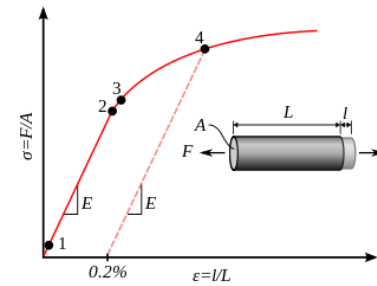
In engineering, the elasticity of a material is quantified by the elastic modulus such as the Young's modulus, bulk modulus or shear modulus which measure the amount of stress needed to achieve a unit of strain; a higher modulus indicates that the material is harder to deform. The material's elastic limit or yield

strength is the maximum stress that can arise before the onset of plastic deformation.

Plasticity (physics):

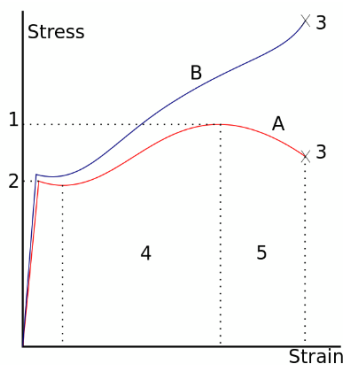
Deformation of a solid material undergoing non-reversible changes of shape in response to applied forces.

In physics and materials science, plasticity, also known as plastic deformation, is the ability of a solid material to undergo permanent deformation, a non-reversible change of shape in response to applied forces. For example, a solid piece of metal being bent or pounded into a new shape displays plasticity as permanent changes occur within the material itself. In engineering, the transition from elastic behavior to plastic behavior is known as yielding.



Stress–strain curve showing typical yield behavior for nonferrous alloys.

1. True elastic limit
2. Proportionality limit
3. Elastic limit
4. Offset yield strength



A stress–strain curve typical of structural steel.

- 1: Ultimate strength
- 2: Yield strength (yield point)
- 3: Rupture

- 4: Strain hardening region
- 5: Necking region
- A: Apparent stress (F/A<sub>0</sub>)
- B: Actual stress (F/A)

Plastic deformation is observed in most materials, particularly metals, soils, rocks, concrete, and foams. However, the physical mechanisms that cause plastic deformation can vary widely. At a crystalline scale, plasticity in metals is usually a consequence of dislocations. Such defects are relatively rare in most crystalline materials, but are numerous in some and part of their crystal structure; in such cases, plastic crystallinity can result. In brittle materials such as rock, concrete and bone, plasticity is caused predominantly by slip at microcracks. In cellular materials such as liquid foams or biological tissues, plasticity is mainly a consequence of bubble or cell rearrangements, notably T1 processes.

For many ductile metals, tensile loading applied to a sample will cause it to behave in an elastic manner. Each increment of load is accompanied by a proportional increment in extension. When the load is removed, the piece returns to its original size. However, once the load exceeds a threshold – the yield strength – the extension increases more rapidly than in the elastic region; now when the load is removed, some degree of extension will remain.

Elastic deformation, however, is an approximation and its quality depends on the time frame considered and loading speed. If, as indicated in the graph opposite, the deformation includes elastic deformation, it is also often referred to as "elasto-plastic deformation" or "elastic-plastic deformation".

Perfect plasticity is a property of materials to undergo irreversible deformation without any increase in stresses or loads. Plastic materials that have been hardened by prior deformation, such as cold forming, may need increasingly higher stresses to deform further. Generally, plastic deformation is also dependent on the deformation speed, i.e. higher stresses usually have to be applied to increase the rate of deformation. Such materials are said to deform viscoplastically.”

#### Viscoelasticity:

Property of materials with both viscous and elastic characteristics under deformation.

In materials science and continuum mechanics, viscoelasticity is the property of materials that exhibit both viscous and elastic characteristics when undergoing deformation. Viscous materials, like water, resist shear flow and strain linearly with time when a stress is applied. Elastic materials strain when stretched and immediately return to their original state once the stress is removed.

Viscoelastic materials have elements of both of these properties and, as such, exhibit time-dependent strain. Whereas elasticity is usually the result of bond stretching along crystallographic planes in an ordered solid, viscosity is the result of the diffusion of atoms or molecules inside an amorphous material.

In the nineteenth century, physicists such as Maxwell, Boltzmann, and Kelvin researched and experimented with creep and recovery of glasses, metals, and rubbers. Viscoelasticity was further examined in the late twentieth century when synthetic polymers were engineered and used in a variety of applications. Viscoelasticity calculations depend heavily on the viscosity variable,  $\eta$ . The inverse of  $\eta$  is also known as fluidity,  $\phi$ . The value of either can be derived as a function of temperature or as a given value (i.e., for a dashpot).

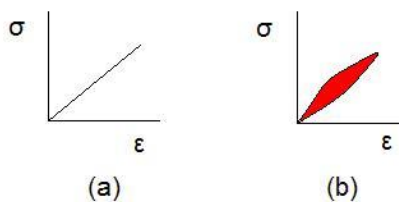
Depending on the change of strain rate versus stress inside a material, the viscosity can be categorized as having a linear, non-linear, or plastic response. When a material exhibits a linear response, it is categorized as a Newtonian material. In this case the stress is linearly proportional to the strain rate. If the material exhibits a non-linear response to the strain rate, it is categorized as non-Newtonian fluid. There is also an interesting case where the viscosity decreases as the shear/strain rate remains constant. A material which exhibits this type of behavior is known as thixotropic. In addition, when the stress is independent of this strain rate, the material exhibits plastic deformation. Many viscoelastic materials exhibit rubber like behavior explained by the thermodynamic theory of polymer elasticity.

Cracking occurs when the strain is applied quickly and outside of the elastic limit. Ligaments and tendons are viscoelastic, so the extent of the potential damage to them depends both on the rate of the change of their length as well as on the force applied.

A viscoelastic material has the following properties:

- hysteresis is seen in the stress–strain curve
- stress relaxation occurs: step constant strain causes decreasing stress
- creep occurs: step constant stress causes increasing strain
- its stiffness depends on the strain rate or the stress rate.

Elastic versus viscoelastic behavior



Stress–strain curves for a purely elastic material (a) and a viscoelastic material (b). The red area is a hysteresis loop and shows the amount of energy lost (as heat) in a loading and unloading cycle. It is equal to

$$\oint \sigma d\epsilon$$

where  $\sigma$  is stress and  $\epsilon$  is strain.

Unlike purely elastic substances, a viscoelastic substance has an elastic component and a viscous component. The viscosity of a viscoelastic substance gives the substance a strain rate dependence on time. Purely elastic materials do not dissipate energy (heat) when a load is applied, then removed. However, a viscoelastic substance dissipates energy when a load is applied, then removed. Hysteresis is observed in the stress–strain curve, with the area of the loop being equal to the energy lost during the loading cycle. Since viscosity is the resistance to thermally activated plastic deformation, a viscous material will lose energy through a loading cycle. Plastic deformation results in lost energy, which is uncharacteristic of a purely elastic material's reaction to a loading cycle.

Specifically, viscoelasticity is a molecular rearrangement. When a stress is applied to a viscoelastic material such as a polymer, parts of the long polymer chain change positions. This movement or rearrangement is called “creep”. Polymers remain a solid material even when these parts of their chains are rearranging in order to accompany the stress, and as this occurs, it creates a back stress in the material. When the back stress is the same magnitude as the applied stress, the material no longer creeps. When the original stress is taken away, the accumulated back stresses will cause the polymer to return to its original form. The material creeps, which gives the prefix visco-, and the material fully recovers, which gives the suffix -elasticity.

Viscoplasticity:

Viscoplasticity is a theory in continuum mechanics that describes the rate-dependent inelastic behavior of solids. Rate-dependence in this context means that the deformation of the material depends on the rate at which loads are applied. The inelastic behavior that is the subject of viscoplasticity is plastic deformation which means that the material undergoes unrecoverable deformations when a load level is reached. Rate-dependent plasticity is important for transient plasticity calculations. The main difference between rate-independent plastic and viscoplastic material models is that the latter exhibit not only permanent deformations after the application of loads but continue to undergo a creep flow as a function of time under the influence of the applied load.

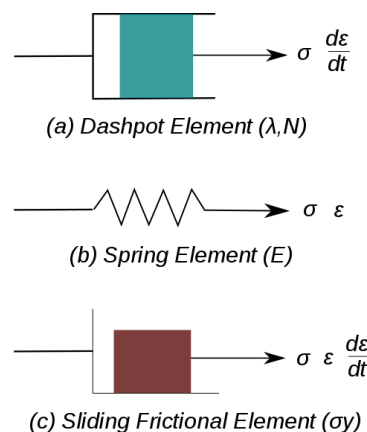


Figure 1. Elements used in one-dimensional models of viscoplastic materials.

The elastic response of viscoplastic materials can be represented in one-dimension by Hookean spring elements. Rate-dependence can be represented by nonlinear dashpot elements in a manner similar to viscoelasticity. Plasticity can be accounted for by adding sliding frictional elements as shown in Figure 1. In the figure  $E$  is the modulus of elasticity,  $\lambda$  is the viscosity parameter and  $N$  is a power-law type parameter that represents non-linear dashpot [ $\sigma(d\epsilon/dt) = \sigma = \lambda(d\epsilon/dt)^{1/N}$ ]. The sliding element can have a yield stress ( $\sigma_y$ ) that is strain rate dependent, or even constant, as shown in Figure 1c.

Viscoplasticity is usually modeled in three-dimensions using overstress models of the Perzyna or Duvaut-Lions types. In these models, the stress is allowed to increase beyond the rate-independent yield surface upon application of a load and then allowed to relax back to the yield surface over time. The yield surface is usually assumed not to be rate-dependent in such models. An alternative approach is to add a strain rate dependence to the yield stress and use the techniques of rate independent plasticity to calculate the response of a material.

For metals and alloys, viscoplasticity is the macroscopic behavior caused by a mechanism linked to the movement of dislocations in grains, with superposed effects of inter-crystalline gliding. The mechanism usually becomes dominant at temperatures greater than approximately one third of the absolute melting temperature. However, certain alloys exhibit viscoplasticity at room temperature (300K). For polymers, wood, and bitumen, the theory of viscoplasticity is required to describe behavior beyond the limit of elasticity or viscoelasticity.

In general, viscoplasticity theories are useful in areas such as

- the calculation of permanent deformations,
- the prediction of the plastic collapse of structures,
- the investigation of stability,
- crash simulations,
- systems exposed to high temperatures such as turbines in engines, e.g. a power plant,

- dynamic problems and systems exposed to high strain rates.

### Phenomenology

For a qualitative analysis, several characteristic tests are performed to describe the phenomenology of viscoplastic materials. Some examples of these tests are

1. hardening tests at constant stress or strain rate,
2. creep tests at constant force, and
3. stress relaxation at constant elongation.

### Strain hardening test

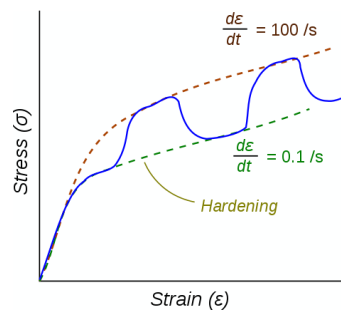


Figure 2. Stress–strain response of a viscoplastic material at different strain rates.

The dotted lines show the response if the strain-rate is held constant. The blue line shows the response when the strain rate is changed suddenly.

One consequence of yielding is that as plastic deformation proceeds, an increase in stress is required to produce additional strain. This phenomenon is known as Strain/Work hardening. For a viscoplastic material the hardening curves are not significantly different from those of rate-independent plastic material. Nevertheless, three essential differences can be observed.

1. At the same strain, the higher the rate of strain the higher the stress.
2. A change in the rate of strain during the test results in an immediate change in the stress–strain curve.
3. The concept of a plastic yield limit is no longer strictly applicable.

The hypothesis of partitioning the strains by decoupling the elastic and plastic parts is still applicable where the strains are small, i.e.,

$$\epsilon = \epsilon_e + \epsilon_{vp}$$

where  $\epsilon_e$  is the elastic strain and  $\epsilon_{vp}$  is the viscoplastic strain.

To obtain the stress–strain behavior shown in blue in the figure, the material is initially loaded at a strain rate of 0.1/s. The strain rate is then instantaneously raised to 100/s and held constant at that value for some time. At the end of that time period the strain rate is dropped instantaneously back to 0.1/s and the cycle is continued for increasing values of strain. There is clearly a lag between the strain-rate change and the stress response. This lag is modeled quite accurately by overstress models (such as the Perzyna model) but not by models of rate-independent plasticity that have a rate-dependent yield stress.”

**Note:** For a more detailed description, please refer to the “consolidated method” section which is given at the beginning of the special issue.

### 3. RESULTS

Figure 1 displays three detailed background information on one chart and the analysis calculation data table.

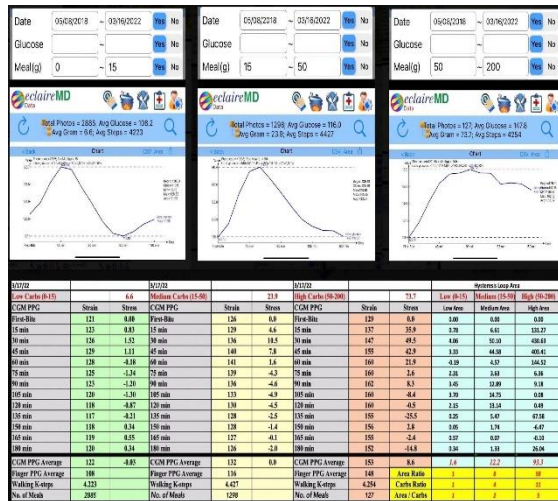


Figure 1: 3 detailed background information chart and analysis calculation data table.

Figure 2 shows three PPG waveforms in a time domain.

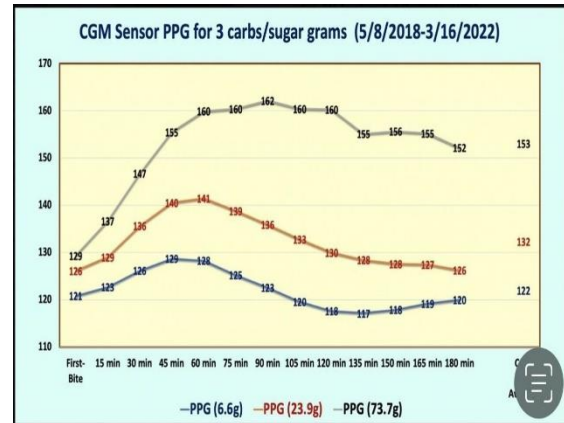


Figure 2: 3 PPG waveforms in a time domain.

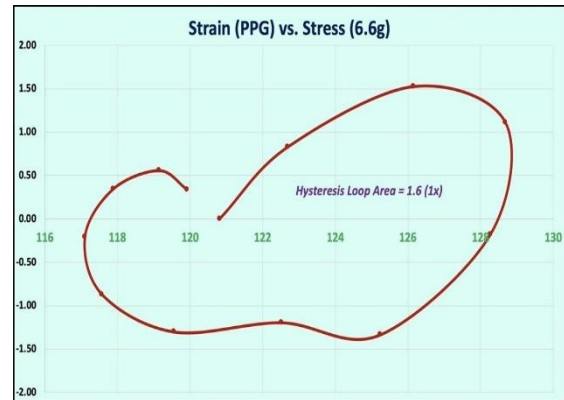


Figure 3: Low PPG sub-groups stress-strain diagrams in a space domain.

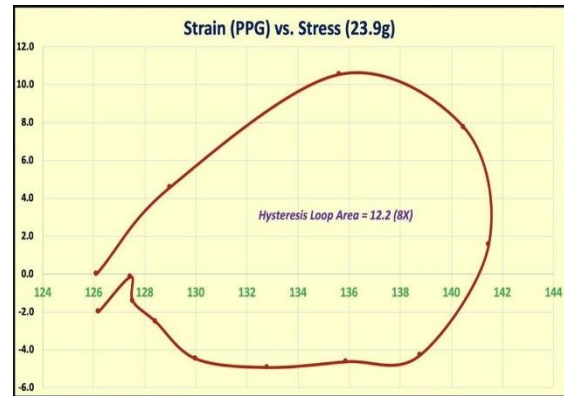


Figure 4: Medium PPG sub-groups stress-strain diagrams in a space domain.

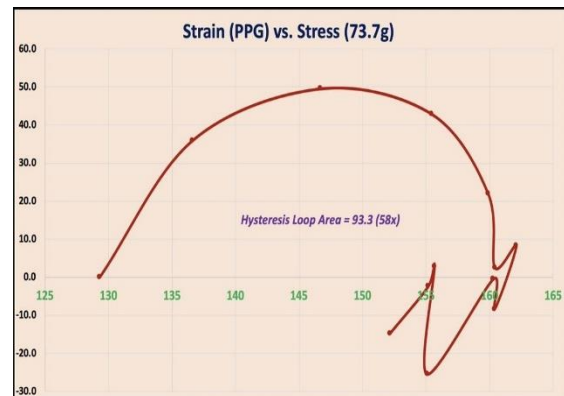


Figure 5: High PPG sub-groups stress-strain diagrams in a space domain.

Figure 6 illustrates a combined chart of the three stress-strain diagrams based on the same scales for the x- and y-axis, along with a ratio table of the loop area, carbs/sugar, and loop area versus carbs/sugar.

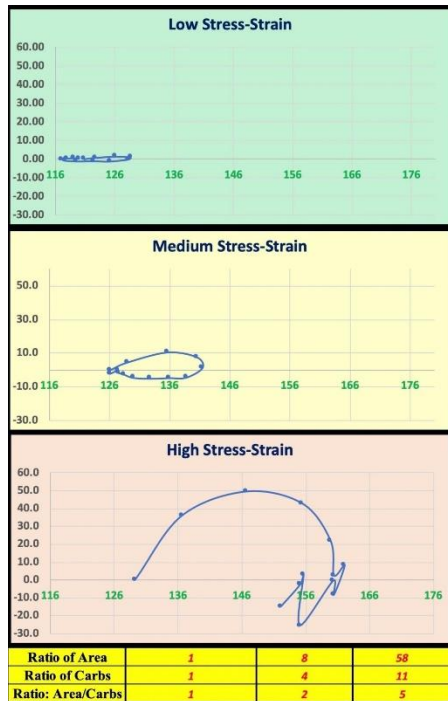


Figure 6: A combined chart of 3 stress-strain diagrams based on the same scales of x- and y-axis, and a ratio table.

#### 4. CONCLUSION

In summary, a clear conclusion can be drawn as follows:

“A higher glucose amount generates higher energy which causes more damage to internal organs through blood flow”. This simple conclusive statement can be easily understood and accepted by medical professionals, except for the word “energy”. However, by using the author’s math-physical medicine (MPM) research methodology, it can offer a concise comprehension of this complex biomedical picture with sound theoretical proof and detailed data.

By delving into this picture closely, we can discover additional findings as explained below. However, the author wants to state the following key conclusive statement first:

“Energy required to cause material failure, such as organ damage, can be represented through the total area under the stress-strain

curve (hysteresis loop) which indicates the energy per unit volume of glucose”.

(1) The low PPG sub-group behaves like an elastic and pseudo viscoelastic pattern since its ending strain (PPG at 120 mg/dL) is almost the same as its starting strain (PPG at 121 mg/dL). Incidentally, the low PPG data are time-dependent. The author selects the extremely low average carbs/sugar intake amount of 6.6 grams from his 2,885 meals (67% of his total 4,310 meals) as its corresponding viscosity factor ( $\eta$ ).

(2) The medium PPG group acts like an elastic and perfect viscoelastic pattern since its ending strain is identical to its starting strain (both PPG at 126 mg/dL). Incidentally, the medium PPG data are also time-dependent. The author selects a higher but moderate average carbs/sugar intake amount of 23.9 grams from his 1,298 meals (30% of his total 4,310 meals) as its corresponding viscosity factor ( $\eta$ ).

(3) The high PPG group behaves like a plastic and viscoplastic pattern since its ending strain (PPG at 152 mg/dL) is much higher than the starting strain (PPG at 129 mg/dL). On the high PPG stress-strain curve, there is a huge opening which is a very different shape from the other two subgroups’ “closed loops”. Even the high PPG data is also time-dependent. The author selects the extremely high average carbs/sugar intake amount of 73.7 grams (3% of his total 4,310 meals) as its corresponding viscosity factor ( $\eta$ ).

(4) From the three separate stress-strain diagrams, we can see three calculated hysteresis loop areas: 1.6 for the low PPG group, 12.2 for the medium PPG group, and 93.3 for the high PPG group. Therefore, combined with the contribution percentage of meals distribution, the total “effective loop area” is:  $1.6 \cdot 0.67 + 12.2 \cdot 0.3 + 93.3 \cdot 0.03 = 1.072 + 3.66 + 2.799 = 7.531$  Energy required to cause material failure, such as organ damage, can be represented through the total area under the stress-strain curve (hysteresis loop) which indicates the energy per unit volume of glucose. This effective loop area of 7.531 is slightly higher than the medium PPG subgroup with 23.9 grams of carbs/sugar and 132 mg/dL of averaged PPG. He should definitely avoid having high PPG (hyperglycemic) situations.

(5) The three comparing ratios for low PPG, medium PPG, and high PPG are: loop area ratios = 1:8:58; carbs/sugar ratios = 1:4:11; ratio of area/carbs = 1:2:5. The three comparisons through different ratios are expressed with a “relative scale of comparison”. It should be noted that the high loop area is caused by the combined effect of the high strain (PPG) and high stress (high PPG change rate with high carbs/sugar), high glucose fluctuation (GF), or high glycemic variability (GV). From the author’s previous research results and other published papers, the high GF or GV indeed causes damage to internal organs.

From the relativity of curve shape, data value, and hysteresis loop area of the individual diagram and the combined chart of the three stress-strain diagrams, the following statement can be made based on the above findings: the high PPG group not only has higher values of PPG, GF, and GV

but also carry a higher level of energy circulating inside the body through blood flow. The high level of energy is the primary source (other than viruses or infections) that cause different types of internal damage to the body organ cells which leads to various chronic disease complications.

## **5. REFERENCES**

For editing purposes, the majority of the references in this paper, which are self-references, have been removed. Only references from other authors' published sources remain. The bibliography of the author’s original self-references can be viewed at [www.eclairemd.com](http://www.eclairemd.com).

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# Viscoelastic and Viscoplastic Glucose Theory Application in Medicine

Gerald C. Hsu

